Microvolt T-Wave Alternans: Physiological Basis, Methods of Measurement, and Clinical Utility
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STATE-OF-THE-ART PAPER

Microvolt T-Wave Alternans

Physiological Basis, Methods of Measurement, and Clinical Utility—Consensus Guideline by International Society for Holter and Noninvasive Electrocardiology

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This consensus guideline was prepared on behalf of the International Society for Holter and Noninvasive Electrocardiology and is cosponsored by the Japanese Circulation Society, the Computers in Cardiology Working Group on e-Cardiology of the European Society of Cardiology, and the European Cardiac Arrhythmia Society. It discusses the electrocardiographic phenomenon of T-wave alternans (TWA) (i.e., a beat-to-beat alternation in the morphology and amplitude of the ST-segment or T-wave). This statement focuses on its physiological basis and measurement technologies and its clinical utility in stratifying risk for life-threatening ventricular arrhythmias. Signal processing techniques including the frequency-domain Spectral Method and the time-domain Modified Moving Average method have demonstrated the utility of TWA in arrhythmia risk stratification in prospective studies in >12,000 patients. The majority of exercise-based studies using both methods have reported high relative risks for cardiovascular mortality and for sudden cardiac death in patients with preserved as well as depressed left ventricular ejection fraction. Studies with ambulatory electrocardiogram-based TWA analysis with Modified Moving Average method have yielded significant predictive capacity. However, negative studies with the Spectral Method have also appeared, including 2 interventional studies in patients with implantable defibrillators. Meta-analyses have been performed to gain insights into this issue. Frontiers of TWA research include use in arrhythmia risk stratification of individuals with preserved ejection fraction, improvements in predictivity with quantitative analysis, and utility in guiding medical as well as device-based therapy. Overall, although TWA appears to be a useful marker of risk for arrhythmic and cardiovascular death, there is as yet no definitive evidence that it can guide therapy. (J Am Coll Cardiol 2011;58:1309–24) © 2011 by the American College of Cardiology Foundation

The International Society for Holter and Noninvasive Electrocardiology together with the Japanese Circulation Society, the Working Group on e-Cardiology of the European Society of Cardiology, and the European Cardiac Arrhythmia Society charged the authors with reviewing the topic of microvolt T-wave alternans (TWA) to provide a consensus guideline with regard to its physiological basis, measurement methods, and clinical utility.

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Physiology of TWA

The TWA phenomenon, a repeating ABABAB pattern in the morphology and amplitude of the ST-segment or T-wave, has long been recognized and linked to arrhythmogenesis (1). This pattern distinguishes TWA from other types of ST-segment and T-wave variability (Fig. 1). TWA reflects spatiotemporal heterogeneity of repolarization, is sensitive to perturbations in intracellular calcium handling, and serves as a mechanism of arrhythmogenesis by amplifying repolarization heterogeneity. It arises from beat-to-beat alternation of action potential duration at the level of cardiac myocytes. TWA can be either spatially concordant, when action potentials in neighboring cell regions alternate in phase, or discordant, when they are out of phase (Figs. 2 and 3) (2,3). The physiological basis of TWA has recently been reviewed in detail (2–7).

Link to repolarization heterogeneity. The association of TWA with spatiotemporal heterogeneity of repolarization (i.e., transient or lasting repolarization differences among neighboring myocardial regions) is supported by a number of investigations, including in vitro optical mapping (2,3,5,7–9), intact large animal experimental laboratory studies (10–13), computer simulations, and clinical studies involving programmed electrical stimulation (14,15). Higher levels of TWA indicate greater risk for arrhythmias (13,16), which becomes especially elevated when alternation in neighboring areas is discordant (i.e., out of phase) (3,10). Changes in action potential duration and conduction velocity restitution, premature beats, and functional and/or anatomic gradients in action potential duration facilitate development of steep, heterogeneous repolarization gradients conducive to re-entry and wavebreak.

Influence of physiological interventions on TWA. TWA magnitude coincides with vulnerability to lethal ventricular tachyarrhythmias. It is amplified by increased heart rates (16), ventricular premature beats (17), coronary artery occlusion and reperfusion (5,12,14,18–20), adrenergic stimulation (18,21), and mental stress (22). Blockade of beta-adrenergic receptors (23,24), sympathetic denervation (18), and vagus nerve and spinal cord stimulation (25), which reduce susceptibility to ventricular tachyarrhythmias, decrease TWA magnitude. Clinical studies with ambulatory electrocardiogram (ECG) monitoring (26) and recordings from intracardiac leads of implanted devices (27) reveal a progressive increase in TWA preceding the onset of spontaneous ventricular arrhythmias.

Heart rate and autonomic factors. Heart rate influences TWA, likely by impacting on intracellular calcium cycling (4) and engaging the steepest portions of the electrical restitution curve (7,28). Even in the normal heart, excessive heart rates of >170 beats/min in guinea pigs and >200 beats/min in canines are capable of inducing TWA (29). During myocardial ischemia or heart failure, the onset heart rate for TWA is considerably lower (9,12) due to impaired capacity of the sarcoplasmic reticulum to reuptake calcium. Heart rate is not the sole determinant of TWA, because autonomic neurotransmitters and changes in myocardial substrate can lead to elevated levels of TWA during fixed rate pacing (16,18). Furthermore, pacing alone does not replicate the TWA enhancement at comparable heart rates due to adrenergic stimulation or myocardial ischemia (21–24).

Myocardial ischemia and heart failure. Myocardial ischemia can increase TWA magnitude, as was evidenced in animals during coronary artery occlusion (16,18,19) and in humans during angioplasty (16,20). Experimental studies with fixed heart rates indicated that myocardial ischemia-
reperfusion-induced increases in TWA magnitude paralleled \( r^2 = 0.98 \) incidence of ventricular tachycardia and fibrillation (16). Marked changes in T-wave complexity and heterogeneity (i.e., nonuniformity in T-wave morphology) (12,13) occurred simultaneously with TWA magnitude surges, with transition from concordant to discordant alternans. Loss of intercellular coupling by ischemia was implicated when rotigaptide decreased connexin43 dephosphorylation in parallel with ischemia-induced TWA and dispersion of repolarization (30).

Derangements in calcium cycling and conduction constitute ionic bases for TWA during myocardial ischemia and heart failure (8,9). With luminescent dyes, Clusin (8) demonstrated ischemia-induced concordant and discordant alternation in calcium transients. Moreover, calcium-channel blockade reversed ischemia-induced TWA in parallel with arrhythmia suppression in anesthetized canines (31). Experimental models of heart failure demonstrated associations of TWA with disturbances in calcium handling and development of discordant alternans, which set up pro-arrhythmic preconditions for conduction block and re-entry. In particular, heart failure reduced sarcoplasmic reticulum calcium ion \( (\text{Ca}^{2+}) \)-adenosine triphosphatase expression and inhibited ryanodine receptor function, resulting in impaired reuptake and release of calcium in the sarcoplasmic reticulum, both contributing to marked derangements in intracellular \( \text{Ca}^{2+} \) handling (9). Recent studies in cardiomyopathy patients showed that TWA may be attributable to oscillations in the action potential plateau that, in computational models, were best explained by reduced calcium uptake into the sarcoplasmic reticulum (15,28).

**TWA in nonischemic cardiomyopathy.** Sympathetic nerve activity and abnormalities in calcium handling may serve as arrhythmogenic factors in nonischemic disease patients, in whom enhanced adrenergic activity compensates for reduced myocardial contractility. The vulnerable myocardial substrate is susceptible to transient alterations in neural activity and electrolyte imbalance, which may initiate disturbances in cardiac repolarization and ventricular arrhythmogenesis. Imaging studies (32) demonstrated the important role of increased sympathetic nerve activity in provoking TWA in idiopathic dilated cardiomyopathy. During exercise, patients with dilated or hypertrophic cardiomyopathy also experience repolarization abnormalities including TWA that are associated with ventricular tachycardia. Histopathological changes, particularly fiber disarray and/or fibrosis, are correlated with TWA.

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**Figure 2** Discordant Alternans Leading to VF

Action potential propagation between 2 ventricular sites (A to B) is shown with transition from concordant to discordant alternans and development of ventricular fibrillation (VF). Shaded areas indicate dispersion of repolarization between sites. *Premature beats. L = long action potential duration; S = short action potential duration. Adapted, with permission, from Oshodi et al. (2).

**Figure 3** Interlead Discordant Alternans

Mid-myocardial (Mid)/epicardial (Epi) recordings after an abrupt decrease in pacing cycle length from 1,000 to 500 ms. Ventricular tachycardia was initiated by a premature focal discharge from a left ventricular endocardial site, which induced areas of functional conduction block and re-entrant excitation. Numbers above the tracing are calculated activation–recovery intervals (ARI). Numbers below the tracing are dispersion of ARI between mid-myocardial and epicardial sites. *Marked discordant alternans is associated with the onset of ventricular tachyarrhythmia after a premature beat. Reprinted, with permission, from Chinushi et al. (3).
### Table 1: Clinical Studies With the Spectral Method Enrolling >100 Patients

<table>
<thead>
<tr>
<th>Predictive studies</th>
<th>Patient Population (Enrollment, Disease)</th>
<th>Mean LVEF</th>
<th>Hazard Ratios (95% CI) for TWA</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Cardiomyopathy</strong></td>
<td><strong>First Author (Ref. #)</strong></td>
<td><strong>Patient Population</strong></td>
<td><strong>Mean LVEF</strong></td>
</tr>
<tr>
<td>Kitamura et al. (34)</td>
<td>104 patients with DCM</td>
<td>37%</td>
<td>11.9 (1.53–92.59) for SCD, VF, or sustained VT at 21 ± 14 months</td>
</tr>
<tr>
<td>Hohnloser et al. (35)</td>
<td>137 patients with DCM, LVEF ≤35%</td>
<td>29 ± 11%</td>
<td>3.44 for ventricular tachyarrhythmic events at 14 ± 6 months</td>
</tr>
<tr>
<td>Chow et al. (36)</td>
<td>514 patients with ischemic cardiomyopathy, LVEF ≤35%, no previous sustained ventricular arrhythmia and positive or indeterminate TWA test results (patients included in Chow et al. [38])</td>
<td>26%–29%</td>
<td>2.24 (1.34–3.75) for all-cause mortality; 2.29 (1.00–5.24) for arrhythmic mortality; NS for nonarrhythmic mortality</td>
</tr>
<tr>
<td>Salerno-Uriarte et al. (ALPHA) (37)</td>
<td>446 patients with DCM, LVEF ≤40%</td>
<td>29.5%</td>
<td>4.0 (1.4–11.4) for cardiac death and life-threatening arrhythmias at 18 months</td>
</tr>
<tr>
<td>Chow et al. (38,39)</td>
<td>768 patients with ischemic cardiomyopathy, LVEF ≤35%, no previous sustained ventricular arrhythmia</td>
<td>26%–29%</td>
<td>2.27 (1.22–4.24) for all-cause mortality in patients without an ICD; 2.42 (1.07–5.41) for all-cause mortality or appropriate ICD discharge in patients with an ICD. ICD use was associated with lower all-cause mortality in MTWA non-negative patients (0.45, 0.27–0.76) but not in MTWA negative patients (0.85, 0.33–2.20), with mortality benefit in MTWA-negative patients largely mediated through arrhythmic mortality reduction (0.30, 0.13–0.68).</td>
</tr>
<tr>
<td>Chan et al. (40)</td>
<td>768 patients with ischemic cardiomyopathy, LVEF ≤35%, no previous sustained ventricular arrhythmia</td>
<td>26%–29%</td>
<td>2.19 (1.1–4.34) for all-cause mortality and appropriate ICD shocks at 1 yr; 3.36 (1.28–8.83) at 2 yrs</td>
</tr>
<tr>
<td>Costantini et al. (ABCD) (41)</td>
<td>566 patients with ischemic cardiomyopathy, LVEF ≤40%, and NSVT</td>
<td>28 ± 8%</td>
<td>2.1 for SCD or appropriate ICD discharge at 1 yr</td>
</tr>
<tr>
<td><strong>Congenital heart disease</strong></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Alexander et al. (42)</td>
<td>304 consecutive pediatric patients with congenital heart disease, myopathy, syncope, or history of cardiac arrest</td>
<td>Not stated</td>
<td>7.9 (2.2–28.1) for ventricular arrhythmia; 6.7 (1.6–28.1) for cardiac arrest at &lt;3 yrs</td>
</tr>
<tr>
<td><strong>Depressed LVEF</strong></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Rashba et al. (43)</td>
<td>108 consecutive patients with CAD and LVEF ≤40%</td>
<td>28 ± 7%</td>
<td>2.2 (1.1–4.7) for death, sustained ventricular arrhythmias, appropriate ICD discharge at 18 ± 13 months in patients with normal QRS segment; NS in patients with prolonged QRS segment</td>
</tr>
<tr>
<td>Rashba et al. (44)</td>
<td>144 patients with CAD and LVEF ≤40%</td>
<td>28 ± 7%</td>
<td>2.2 (1.1–4.7) for death, sustained ventricular arrhythmia, or appropriate ICD discharge at 17 ± 13 months; NS in patients with LVEF &lt;30%; in patients with LVEF &gt;30%</td>
</tr>
<tr>
<td>Bloomfield et al. (45)</td>
<td>549 patients with LVEF ≤40%, no history of sustained ventricular arrhythmias</td>
<td>25%</td>
<td>6.5 (2.4–18.1) for all-cause mortality or nonfatal sustained ventricular arrhythmia at 2 yrs</td>
</tr>
<tr>
<td>Cantillon et al. (46)</td>
<td>286 patients with LVEF ≤35%, NSVT or syncope</td>
<td>26 ± 7%</td>
<td>2.33 (1.44–3.67) for arrhythmia-free survival at 38 ± 11 months</td>
</tr>
<tr>
<td>Morin et al. (47)</td>
<td>386 patients with CAD, NSVT, LVEF ≤40%</td>
<td>26%–30%</td>
<td>1.64 for ventricular tachyarrhythmia or death in patients with narrow QRS segment at 40 ± 19 months; NS in patients with wide QRS segment</td>
</tr>
<tr>
<td><strong>Heart failure</strong></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Klingengeben et al. (48)</td>
<td>107 consecutive patients with congestive heart failure, LVEF ≤45%, no history of arrhythmia, and no recent MI</td>
<td>28 ± 7%</td>
<td>for SCD, arrhythmias, sustained VT at 14.6 months</td>
</tr>
<tr>
<td>Gorodeski et al. (49)</td>
<td>303 consecutive patients with heart failure and LVEF ≤40%</td>
<td>24%</td>
<td>1.89 (1.05–3.39) for total mortality or cardiac transplantation; NS after adjustment for metabolic measures at 2.8 yrs. Concordance index for time-to-event outcomes = 0.75. C statistic for propensity score = 0.79.</td>
</tr>
</tbody>
</table>

Continued on next page
occurrence and ventricular tachyarrhythmias in hypertrophic cardiomyopathy (33).

**Methodology for TWA Assessment**

Two contemporary techniques employed in sizable clinical studies for arrhythmia risk stratification by microvolt-level TWA are the Spectral and the Modified Moving Average (MMA) Methods (Tables 1 and 2) (34–74). Both allow detection of subtle levels of TWA in the nonvisible microvolt range as well as visible, macroscopic TWA. Experience with the Spectral Method is more extensive. Other analytical methods employed in experimental and clinical studies (18,20,26,75,76) have been reviewed (75).

**Spectral Method. ANALYSIS APPROACH.** The concept of analyzing morphology fluctuations in the T-wave by computerized spectral techniques dates from experimental studies (29) employing the Fast Fourier Transform (FFT) (Fig. 4) (77). In detail, sequential ECG cycles are aligned to their QRS complex, and the amplitude of the ST segments and T waves at 128 pre-defined points \( t \) (relative to the JT interval) is measured. Subsequently, each beat-to-beat series of amplitude fluctuations is processed with FFT to generate a separate spectrum for each point \( t \). The spectra corresponding to different time points along the JT interval are averaged, producing a composite spectrum. The voltage difference between the overall mean beat and the even- or odd-numbered mean beats, or the alternans voltage in microvolts, represents the square root of the alternans power at 0.5 cycle/beat.

The significance of TWA is expressed by the alternans ratio (K score), calculated as the ratio of alternans power at 0.5 cycle/beat divided by the standard deviation of spectral noise (78). The greater the power, the higher is the alternans voltage. The ECG fluctuations occurring at other frequencies are not included in...
Institutes of Health, Bethesda Maryland) and Paperchase (Bedford Massachusetts) databases. Reference lists from these studies and from recent reviews (4–7) were also scanned.

This table is based on searches of the published medical data on the terms alternans and alternation for all clinical studies that reported hazard ratios in PubMed (National Library of Medicine, National Clinical Studies) With the Modified Moving Average Method

### Table 2 Clinical Studies With the Modified Moving Average Method

<table>
<thead>
<tr>
<th>Test Setting</th>
<th>Patient Population</th>
<th>Mean LVEF</th>
<th>Hazard Ratios (95% CI) for TWA; NPV and PPV</th>
</tr>
</thead>
<tbody>
<tr>
<td>Routine exercise testing</td>
<td>Nieminen et al. (FINCAVAS) (64)</td>
<td>Mostly preserved</td>
<td>6.0 (2.8–12.8) for CV death, 7.4 (2.8–19.4) for SCD at 44 ± 7 months for 65-μV TWA cutpoint; NPV for CV death = 97.6; PPV = 11.6; NPV for SCD = 98.6, PPV = 8.0</td>
</tr>
<tr>
<td></td>
<td>Minkkinen et al. (FINCAVAS) (65)</td>
<td>Mostly preserved</td>
<td>4.6 (2.2–9.9) for CV death, 4.4 (1.5–12.7) for SCD at 47 months for 65-μV cutpoint; NPV for CV death = 97.4; PPV = 10.2</td>
</tr>
<tr>
<td></td>
<td>Leino et al. (FINCAVAS) (66)</td>
<td>Mostly preserved</td>
<td>1.55 (1.150–2.108, p &lt; 0.004) for CV death; 1.58 (1.041–2.412; p &lt; 0.033) for SCD at 55 months per 20 μV TWA in lead V2.</td>
</tr>
<tr>
<td>Exercise recovery</td>
<td>Exner et al. (REFINE) (54)</td>
<td>Moderately depressed (38%–48%)</td>
<td>2.94 (1.10–7.87) monitored at 10–14 weeks after event for CV death or resuscitated cardiac arrest (primary endpoint) at 47 months; NS when monitored at 2–4 weeks after MI. For primary endpoint for TWA, AUC = 0.62; for combination of TWA + HRT, AUC = 0.71.</td>
</tr>
<tr>
<td></td>
<td>Slawnych et al. (REFINE/FINCAVAS) (67)</td>
<td>Moderately depressed (38%–48%) and preserved (56%–63%) groups</td>
<td>2.5 (1.1–6.0) for CV death at 48 months for 60-μV cutpoint; NPV = 96%; PPV = 13%. AUC for CV mortality = 0.69.</td>
</tr>
<tr>
<td></td>
<td>Leino et al. (FINCAVAS) (68)</td>
<td>Mostly preserved</td>
<td>3.5 (1.6–7.9) for CV death at 48 months for 60-μV cutpoint. For CV death for TWA alone, C-statistic = 0.550–0.606; for combination of TWA + HRR, C-statistic = 0.671–0.691.</td>
</tr>
<tr>
<td>Ambulatory ECG monitoring</td>
<td>Verrier et al. (ATRAMI) (69)</td>
<td>Moderately depressed (42 ± 3%)</td>
<td>7.9 (1.9–33.1) for cardiac arrest or arrhythmic death at 21 months for a priori 75th percentile cutpoint (47 μV); patients were monitored at 15 ± 10 days post-MI.</td>
</tr>
<tr>
<td></td>
<td>Stein et al. (EPHESUS) (70)</td>
<td>Depressed (34 ± 5%)</td>
<td>5.5 (2.2–13.8) for SCD at 16.4 months for 47-μV cutpoint; patients were monitored at 2–10 days post-MI. For SCD, AUC = 0.73 for TWA in lead V2 and = 0.70 in lead V3 (p &lt; 0.001).</td>
</tr>
<tr>
<td></td>
<td>Sakaki et al. (71)</td>
<td>Depressed (34 ± 6%)</td>
<td>17.1 (6.3–46.6) for CV death, 22.8 (2.6–193.7) for witnessed SCD at 1 yr for 65-μV cutpoint; NPV for CV death = 97%; PPV = 37%</td>
</tr>
<tr>
<td></td>
<td>Maeda et al. (72)</td>
<td>Depressed (36%–43%) for post-MI group</td>
<td>6.1 (1.1–34.0) for sustained VT or VF at 6 yrs for 65-μV cutpoint</td>
</tr>
<tr>
<td></td>
<td>Stein et al. (CHS) (73)</td>
<td>Not tested, assumed preserved</td>
<td>4.8 (1.48–15.81) for SCD at 14 yrs</td>
</tr>
<tr>
<td></td>
<td>Hou et al. (74)</td>
<td>&gt;35% in 201; ≤35% in 18</td>
<td>17.78 (3.75–84.31) for SCD within 16 months for 47-μV cutpoint; patients were monitored at 1–15 days post-MI; NPV = 99%; PPV = 17%</td>
</tr>
</tbody>
</table>

This table is based on searches of the published medical data on the terms alternans and alternation for all clinical studies that reported hazard ratios in PubMed (National Library of Medicine, National Institutes of Health, Bethesda Maryland) and Paperchase (Bedford Massachusetts) databases. Reference lists from these studies and from recent reviews (4–7) were also scanned.

ATRAMI = Autonomic Tone and Reflexes after Myocardial Infarction; CHS = Cardiovascular Health Study; CV = cardiovascular; EPHESUS = Eplerenone Post-Acute Myocardial Infarction Heart Failure Efficacy and Survival Study; FINCAVAS = Finnish Cardiovascular Study; HRR = heart rate recovery; NPV = negative predictive value; PPV = positive predictive value; other abbreviations as in Table 1.
TWA assessment. Use of this technique in clinical practice is evidenced by substantial sales of commercial equipment and consumables as publicly reported by Cambridge Heart, Inc.

**TEST METHODOLOGY.** Because the Spectral Method involves a graded increase in heart rate, the TWA test is usually conducted during bicycle or treadmill exercise to an optimum heart rate (79). Some investigators infused chronotropic agents (21,24) or employed atrial pacing to elevate and stabilize heart rate (23,56–82). TWA can occur in normal individuals at heart rates >110 beats/min. Consequently, a target heart rate range of 105 to 110 beats/min was determined for pathologic alternans in adults (78,82). Practice has varied with regard to withholding beta-adrenergic blockade to allow patients to reach this heart rate (83). The current recommendation is to maintain chronic medications during the test (23).

TWA is determined from standard precordial and orthogonal X,Y,Z leads. Special high-resolution electrodes can minimize noise. TWA is not measured in ECG portions in which ectopic or premature beats constitute >10% of beats (78), because the readings can be influenced by excessive numbers of premature beats or by attendant phase changes of alternans (e.g., from “ABAB” to “BABA”).

**CLASSIFICATION OF TEST RESULTS.** TWA level >1.9-μV cutpoint with alternans signal-to-noise ratio K >3 sustained for >2 min is defined as a positive test result on the basis of outcome data of clinical studies (55,78). Test results below this level are considered negative.

Because of a relatively high incidence (20% to 40% of all cases) of indeterminate test results, a test classification of “abnormal due to patient factors” was introduced (84). This classification is employed when the test is associated with excessive ectopy (approximately 32%), lack of capacity to reach a target rate of 105 to 110 beats/min (approximately 51%), or nonsustained TWA (approximately 10%). Abnormal test results due to patient factors carry greater risk than positive test results. In contrast, the occurrence of muscle, respiration, or other movement artifacts or electrode noise accounts for 6.4% of indeterminate test results in experienced centers and is referred to as “technically indeterminate.” Those tests have no prognostic value per se.

**MMA method. ANALYSIS APPROACH.** The MMA method employs the noise-rejection principle of recursive averaging (75). The algorithm continuously streams odd and even beats into separate bins and creates median complexes for each bin (Fig. 5) (19). These complexes are then superimposed, and the maximum difference between the odd and even median complexes at any point within the JT segment is averaged for every 10 to 15 s and reported as the TWA value. The moving average allows control of the influence of new incoming beats on the median templates with an adjustable update factor (i.e., the fraction of morphology...
change that an incoming beat can contribute). The recommended rapid update factor of one-eighth provides greater sensitivity and capacity to detect transient but clinically important surges in TWA than one-sixteenth or one-thirty-second (64). Noise measurements are in part derived from mismatch of the even or odd median complexes outside the JT segment. The algorithm excludes extrasystoles, noisy beats, and the beats preceding them and filters effects of noise, movement, and respiration.

**TEST METHODOLOGY.** The MMA allows microvolt TWA analysis during routine, symptom-limited exercise stress testing (64–66,68) and during post-exercise recovery (54,67,68) as well as during ambulatory ECG monitoring (69–74) in the flow of clinical evaluation (Table 2). Risk stratification is based on the peak TWA value throughout the 24-h ambulatory ECG recording or the symptom-limited exercise test.

MMA-based TWA is calculated from standard precordial ECG leads with standard electrodes (64–74). Because limb leads are prone to motion artifact (65), TWA in these leads should be interpreted with caution. The MMA method generates high-resolution templates of superimposed QRS-aligned complexes showing the alternation pattern, which permit visual examination to verify the presence and magnitude of TWA (Fig. 1) (65,70). TWA values should be over-read for verification down to 20 μV.

**CLASSIFICATION OF TEST RESULTS.** MMA-based TWA studies with ambulatory ECG recordings and exercise support the concept that TWA represents a continuum of risk with higher TWA levels indicating greater risk (64–68). With the recommended update factor of one-eighth, TWA ≥60 μV during routine exercise testing (64–68) and ambulatory ECG monitoring (69–74) indicates severely elevated risk for sudden cardiac death and/or cardiovascular mortality. In patients during the early post-MI phase with or without heart failure, a cutoff point of ≥47 μV also predicted sudden cardiac death (69,70,74). Leino et al. (66) demonstrated a 55% and 58% increase in risk of cardiovascular and sudden cardiac death, respectively, per 20 μV of TWA.

**Short- and long-term repeatability of TWA testing.** Immediate repeatability of the Spectral Method test results was verified with bicycle ergometry with 15 min and 4 h between the tests (85) as well as during atrial pacing (24). Data on long-term stability of TWA results with the Spectral Method are sparse (86). Repeatability has not been reported with the MMA method.

**Comparison of TWA values obtained with the Spectral and MMA methods.** The methods are analytically comparable, although they differ in noise processing. The 4- to 10-fold differences in TWA voltages reported by MMA and Spectral Method tests can be accounted for by the update factor (87). Also, the Spectral Method reports one-half of the average TWA magnitude across the entire JT interval for 128 beats, whereas the MMA method reports the peak TWA level at any point within the JT interval for each 10- to 15-s interval.

**Clinical Utility**

**Spectral Method.** Significant predictivity of TWA analysis by the Spectral Method has been prospectively demonstrated in >7,200 patients with various types of cardiovascular disease, including myocardial infarction, congestive heart failure, ischemic cardiomyopathy, and nonischemic dilated cardiomyopathy (Table 1) (Figs. 6A and 6B) (37,54). Lack of significant predictivity in a few observational studies has been attributed to short periods after myocardial infarction during ongoing remodeling (57,58), washout of beta-blocking agents before the test (23,59,83), and use of implantable cardioverter-defibrillator (ICD) firing as a surrogate endpoint for arrhythmic death (61,62,88).

A focus of most TWA studies with the Spectral Method has been on identifying patients who would not benefit from ICD implantation, particularly those fulfilling the MADIT II (Multicenter Automatic Defibrillator Trial II) criteria,
namely, prior myocardial infarction and left ventricular ejection fraction (LVEF) ≤30% (52,62). The need for accurate identification of patients who would not benefit from ICD implantation is underscored by the facts that one-third of ICD patients receives an inappropriate shock within 1 to 3 years of implantation (89,90), and ICD shock is associated with a 2- to 5-fold increase in mortality, most commonly due to progressive heart failure (90). Event-free survival from all-cause or cardiac mortality and/or ventricular tachyarrhythmias averaged 97% to 98% in patients with negative TWA test results, pointing to a potential to improve exclusion of patients who may not benefit from primary prophylactic ICD implantation, despite meeting evidence-based criterion of LVEF ≤35% (52,91).

TWA IN INTERVENTIONAL ICD TRIALS. TWA stratified total mortality in the MASTER (Microvolt T Wave Alternans Testing for Risk Stratification of Post-Myocardial Infarction Patients) trial of MADIT II-type patients but did not predict sudden cardiac death or appropriate ICD discharge in the MASTER trial (62) or sudden cardiac death, sustained ventricular tachycardia or fibrillation, or appropriate ICD discharge in the SCD-HeFT (Sudden Cardiac Death in Heart Failure Trial) TWA substudy (Fig. 6C) (61). A recent meta-analysis addressing lack of predictivity of ICD discharge in these trials indicated that predictive accuracy was strong in the TWA studies enrolling relatively few patients with ICDs, with a composite hazard ratio for prediction by abnormal versus negative TWA of 13.6 (95% confidence interval [CI]: 8.5 to 30.4) and that predictive accuracy in studies with high ICD use was low at 1.6 (95% CI: 1.2 to 2.1) (88). Thus, ICD firing, employed as a surrogate endpoint for sudden cardiac death, may have underrepresented the utility of the test. An alternative explanation implicates withholding beta-adrenergic blocking agents to explain the inconsistent results (Fig. 7) (83).

GUIDING ICD IMPLANTATION. Data to support use of TWA to withhold or delay ICD implantation are insufficient at present. To date, only the ABCD (Alternans Before
Cardioverter Defibrillator) trial (41) has tested the capacity of TWA to guide prophylactic ICD implantation. Event rates were higher in patients with either a positive TWA (hazard ratio: 2.1, p = 0.03) or a positive electrophysiological study (hazard ratio: 2.4, p = 0.007) than in those whose TWA and electrophysiological tests were either negative or indeterminate at the pre-specified primary time point of 1 year. Moreover, the event rate in patients with both negative TWA and electrophysiological study test results was lower than in patients with 2 positive tests (2% vs. 12%; p = 0.017), suggesting synergy between the tests. But, TWA did not predict endpoint events at 2 years, suggesting potential time dependence.

In their meta-analysis, Hohnloser et al. (88) proposed a clinical algorithm to identify patients who would not benefit from ICD implantation for primary prevention. Their analysis revealed that the mortality rate of TWA negative patients with LVEF ≤35% but no history of ventricular arrhythmias and no prior ICD implantation was 4-fold lower than that of MADIT II or SCD-HeFT trial patients randomized to ICD therapy. Accordingly, the negative predictive value derived for this group is >99%. This algorithm will require testing in a prospective trial.

TWA IN HEREDITARY CHANNELOPATHIES. Although intracardiac repolarization alternans plays a pivotal pathogenetic role in the genesis of malignant arrhythmias, particularly torsades de pointes, in channelopathies (92), prospective studies have not demonstrated that TWA analysis by the Spectral Method identifies patients with long QT (93,94) or Brugada syndromes (60,95) who will experience episodes of torsades de pointes. The disappearance of TWA during atrial pacing at 110 beats/min provides clues with regard to difficulties in sensing TWA during target heart-rate exercise in Brugada patients (96).

MMA method. Predictivity of TWA analysis by the MMA method has been demonstrated in >4,800 patients, including those with coronary artery disease, recent or old myocardial infarction, congestive heart failure, or cardiomyopathy (Table 2). In FINCAVAS (Finnish Cardiovascular Study), the largest investigation of TWA to date, TWA predicted sudden cardiac death and cardiovascular and total mortality in a general population of >3,500 low-risk patients referred for routine, symptom-limited exercise testing (64–66,68). MMA-based TWA is also predictive when monitored during immediate post-exercise recovery (54,67,68) or from ambulatory ECG records (69–74).

Figure 7 Beta-Blocker TWA Meta-Analysis

Association between microvolt TWA analyzed by the Spectral Method and ventricular arrhythmic events, stratified by screening protocol discontinuation of beta-blocker therapy. Washout of beta-adrenergic blockade impaired predictivity. Risk ratio (RR): 12.44 reflects 0.5 correction factor; therefore, no 95% CI is depicted. *Study estimates for meta-analysis were hazard or risk ratios. **No events in microvolt TWA negative group (p = 0.04). ***Test for heterogeneity: p = 0.025. Abbreviations as in Table 1. Reprinted, with permission, from Chan et al. (83).
(Fig. 6D). Sudden cardiac death was witnessed (71) or judged by physician review (68,73,97) or an events committee (98,99). TWA detected with continuous 24-h ECG monitoring reflects the influences of daily activity, mental stress (22), sleep states (100), and sleep apnea (101). Results of these investigations support MMA analysis of TWA during the flow of routine clinical assessment.

Comparison of the predictivity of TWA with the Spectral and MMA methods. Hazard ratios for prediction by the Spectral and MMA methods are similar, whether in the same population (54) or in studies overall (Tables 1 and 2). Exner et al. (54) determined that TWA assessed by the Spectral Method during exercise and by the MMA method during the post-exercise recovery phase yielded significant odds ratios of 2.75 and 2.94, respectively, in 322 post-myocardial infarction patients with better-preserved LVEF (mean 47% measured at 8 weeks after myocardial infarction) but without an ICD who were enrolled in the REFINE (Risk Estimation Following Infarction, Noninvasive Evaluation) study (Fig. 6B). The concordance of the 2 methods measured simultaneously during exercise has not been systematically investigated. In a study using atrial pacing (n = 41), Cox et al. (80) found that the Spectral Method was predictive (p < 0.02) and that, with their customized software and with one-sixteenth rather than the recommended one-eighth update factor, MMA was nearly significant (p = 0.06) in the same patients. TWA analyzed by both the Spectral Method and MMA was significantly elevated at 8 to 15 min before the onset of spontaneous ventricular tachyarrhythmias in ambulatory ECGs in the ESVE (Electrophysiologic Study Versus Electrocardiographic Monitoring) trial (26).

Risk stratification in patients with preserved ejection fraction. An important frontier in arrhythmia risk stratification concerns patients with preserved LVEF, in whom the majority of sudden cardiac deaths occur albeit with low incidence (102). Ikeda et al. (53) with the Spectral Method and the FINCAVAS investigators (64–68) with the MMA method showed that TWA can identify individuals with preserved LVEF but heightened risk for sudden cardiac death. Positive predictivity in this population is relatively low, in the 8% to 10% range, typical for prognostic markers applied to low-risk groups.

Combinations of noninvasive parameters to improve risk stratification. Improved risk stratification in patients with preserved LVEF can be attained by a combination of noninvasive markers, because the capacity to detect risk increases markedly when more than 1 factor is analyzed (103). Hazard ratios increased by 30% to 212% (54,68) and increases markedly when more than 1 factor is analyzed. Use of combinations of noninvasive parameters, specifically including TWA, was recently recommended in a National Heart, Lung, and Blood Institute and Heart Rhythm Society Workshop report on sudden cardiac death prediction and prevention (104), citing complexities of myocardial substrates underlying sudden cardiac death risk. However, high levels of TWA even in the absence of additional risk markers should be noted.

Quantitative analysis of TWA voltage. GRADED ASSESSMENT OF RISK. To date, most TWA studies have employed a binary approach to classify test results as either negative or abnormal on the basis of a cutpoint. However, because TWA reflects a continuum of cardiac electrical instability, its quantification offers the potential for diagnosing levels of risk and for improving prognostics. Treating a continuous variable as binary reduces predictive power by one-third to one-half (105).

Clinical studies using either the Spectral (26,106) or MMA methods (26,64–68) reveal that higher TWA magnitudes indicate increased risk for ventricular tachyarrhythmias. Klinghenbeben et al. (106) found in patients with infarct-related or nonischemic cardiomyopathy that TWA magnitude and not merely its presence was associated with tachyarrhythmic complications. In the FINCAVAS database, Minkinnen et al. (65), Slawnych et al. (67), and Leino et al. (66) reported that sudden cardiac death incidence and cardiovascular and total mortality rose with elevated TWA values (Fig. 8) (67). Leino et al. (66) determined that risk for cardiovascular death and sudden cardiac death increased by 55% and 58%, respectively, for each 20 μV of TWA. A crescendo in TWA magnitude consistently occurred before onset of life-threatening ventricular tachyarrhythmias in ambulatory subjects with ischemic heart disease enrolled in the ESVE (Electrophysiologic Study Versus Electrocardiographic Monitoring) trial (26). During the arrhythmia-free period, TWA was significantly lower than during the...
Quantitative TWA analysis may allow tracking changes in risk over time, as patients recover and the myocardium remodels, as cardiac disease or heart failure status are altered, or in response to medical therapy. TWA quantification also permits comparison of risk levels across different populations and disease states. For example, it was recently shown that TWA is markedly elevated (≥60 μV) in dialysis patients in the absence of an acute cardiovascular event, consistent with their established heightened risk for sudden cardiac death (107).

GUIDING MEDICAL THERAPY. Clinical studies and reports suggest that the magnitude of TWA reflects the effects of pharmacologic therapy without reducing the predictive capacity of the phenomenon (108). Beta-adrenergic (23,24,83) and sodium channel blocking agents (109) diminish TWA magnitude, reflecting the capacity of these agents to reduce sudden cardiac death and cardiovascular mortality (110). In the Brugada syndrome, sodium channel blockade provokes the diagnostic ECG changes as well as macroscopic TWA and arrhythmias (111). The proarhythmic effects associated with cardiovascular and noncardiovascular agents are also disclosed by elevated levels of TWA.

Because antiadrenergic and antiarrhythmic drugs influence TWA, the decision to withhold these agents at the time of TWA testing is a matter of debate. Some investigators withheld beta-blocker therapy to avoid drug-induced chronotropic incompetence (36,38,39,41,61,62), whereas others performed the test with full cardioprotective medication (35,37,45,48). In a meta-analysis, Chan et al. (83) determined that the predictive capacity of TWA for ventricular arrhythmic events was significantly weaker in studies withholding beta-blockade therapy (relative risk: 1.40; 95% CI: 1.06 to 1.84; p = 0.02) than in studies performed with discharge medications (relative risk: 5.39; 95% CI: 2.68 to 10.84; p < 0.001) (Fig. 7). An important corollary of these findings is that the effects of medications on TWA represent not a disruption in measurement but an indication of therapeutic efficacy (108).

Summary and Recommendations for Clinical Practice

An extensive body of evidence from prospective studies in >12,000 patients with depressed or preserved LVEF supports the use of TWA analysis in assessing risk for cardiovascular mortality and sudden cardiac death (Tables 1 and 2) (112). Hazard ratios generated by the Spectral and MMA methods are similar, whether in the same population (54) or in studies overall. Multivariate analyses confirm that TWA provides information on risk beyond standard clinical variables for cardiovascular disease, including demographic factors (e.g., age, sex, and race) and traditional cardiovascular risk markers (e.g., smoking, blood pressure, history, and medications). Currently, the only established risk marker for sudden cardiac death and the only parameter approved to identify high-risk patients for ICD implantation is depressed LVEF (113). This parameter has significant limitations, as underscored by the fact that the majority of individuals who die suddenly have preserved LVEF (102). TWA is being assessed along with candidate genes as arrhythmia markers in a large cohort of patients with ICDs for ICD shock risk and mortality in EUTrigTreat (EU TrigTreat Clinical Study: An Arrhythmia Risk Stratification and Genetic Trial) (Clinical trials identifier: NCT01209494) and in the GAME (Medtronic Genetic Arrhythmia Markers for Early Detection) study (Clinical trials identifier: NCT00664807).

Accordingly, we concur with the recommendations of guidelines committees of the American Heart Association, American College of Cardiology, European Society of Cardiology, and/or Heart Rhythm Society chaired by Zipes et al. (114), who assigned Class I Level of Evidence: A and Class IIa Level of Evidence: A indications to TWA testing for arrhythmia risk, and led by Goldberger et al. (115), who determined that TWA provides valuable information with regard to risk for cardiovascular mortality and sudden cardiac death. Additional applications recommended by task force or consensus statement authors are in neonates, in whom the appearance of TWA signals the highest level of risk (116), and in hospital settings to warn of the development of torsade de pointes (117).

Interventional trials, which have been performed to date only with the Spectral Method, have not demonstrated that a negative TWA test result can sufficiently guide decision-making with regard to ICD implantation (41,61,62). Thus, TWA should not be used as a sole parameter either to rule in or to rule out ICD use. A clinical algorithm that incorporates LVEF in the decision-making process appears promising on the basis of a meta-analysis (88). However, this proposal will require prospective testing. Also, use of more advanced statistical approaches and criteria for evaluation of novel markers of cardiovascular risk is recommended (118).

Acknowledging the complexities of myocardial substrates underlying sudden cardiac death risk, a recent National Heart, Lung, and Blood Institute and Heart Rhythm Society Workshop report on prediction and prevention proposed combinations of risk markers specifically including TWA (104). The utility of ambulatory TWA combined with heart rate turbulence, an indicator of baroreceptor sensitivity (119), to identify post-myocardial infarction patients with preserved LVEF who would benefit from ICD implantation is the subject of an ongoing clinical trial, REFINE-ICD (Risk Estimation Following Infarction, Noninvasive Evaluation of ICD Therapy) (120) (Clinical trials identifier: NCT00673842).

 identifier: NCT00589849). Exner et al. (54) determined that, for long-term prediction, TWA testing should be performed at 10 to 14 weeks after myocardial infarction, while others (69,70,74) found significant risk stratification with TWA monitoring at ≤15 days post-MI. There is a rationale for considering earlier TWA testing, because 1.4% of patients (approximately 17,500 in the United States) experience sudden cardiac death in the first month after myocardial infarction during the acute remodeling period (121).

Evidence supports the value of quantitative TWA analysis for both the Spectral and MMA methods. Quantification offers inherent advantages with respect to gauging level of risk across time after cardiovascular events and in evaluation of the potential anti- and pro-arrhythmic effects of medical therapy by conventional and nonconventional agents (108). These applications merit exploration in interventional trials.

It is recommended that TWA testing be performed on discharge medications, particularly with respect to beta-blockade therapy (23,83), to ensure that the test results reflect the effects of chronic drug therapy.

Conclusions

Overall, our assessment is that it is reasonable to consider TWA evaluation whenever there is suspicion of vulnerability to lethal cardiac arrhythmias. However, there is as yet no definitive evidence from interventional trials that it can guide therapy.

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Microvolt T-Wave Alternans: Physiological Basis, Methods of Measurement, and Clinical Utility

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